

**The Relevance of Dose
for
Low-Energy Beta Emitters**

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**EU Scientific Seminar
Emerging Issues on Tritium and Low Energy Beta Emitters**

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OUTLINE

Introductory comments on dose, radiation quality and RBE

ICRP system

Some issues for this symposium

Beta-decay of radionuclides
Low-energy beta emitters

Unusual features of low-energy beta emitters

A few additional comments

Conclusions and recommendations

Introductory comments on 'Dose' (and radiation quality)

Absorbed Dose

- Physical quantity, precisely defined, no changeable parameters
- Absorbed dose is the quotient of d_e by dm , where d_e is the mean energy imparted to matter of mass dm .
- Absorbed dose = Deposited Energy \div Mass **$D = d_e/dm$**
- Units: joule per kilogram = gray (Gy)

- Independent of type (quality) of ionizing radiation
- Approximately proportional to the average density of ionizations in the mass (volume) of interest

BUT biological effectiveness of a given absorbed dose depends on many additional factors, including:

- Type of radiation (i.e. radiation quality)
- Dose rate, dose fractionation
- Particular biological system, effect and level of interest

This symposium is particularly concerned with radiation quality

- **of tritium (^3H) and other low-energy beta emitters, that is, with low energy electrons;**
- **and comparison with reference radiations, that is, mixed high- and low-energy electrons from gamma-rays or orthovoltage X-rays;**

Also some additional special features of these beta emitters.

Radiation quality

Determined by the track structure of the radiation

- **Microscopic features of the individual tracks**
- **Relationship between separate tracks, in time and space.**

(1)

Low-LET tracks
in cell nucleus
e.g. from γ -rays



A dose of 1 Gy
corresponds to
 ~ 1000 tracks

(2)



High-LET tracks
in cell nucleus
e.g. alpha-particles

A dose of 1 Gy
corresponds to
 ~ 4 tracks

$\sim 1 \mu\text{m}$

Cell nucleus

Low-LET reference radiation:

Sparsely ionizing on average,
but $\sim 1/4$ of energy deposited via
denser clusters of ionizations
from low-energy secondary
electrons (on scale of nanometres)
(Magnified in diagram)

Very low dose from a single track
(ave ~ 0.001 Gy to cell nucleus)

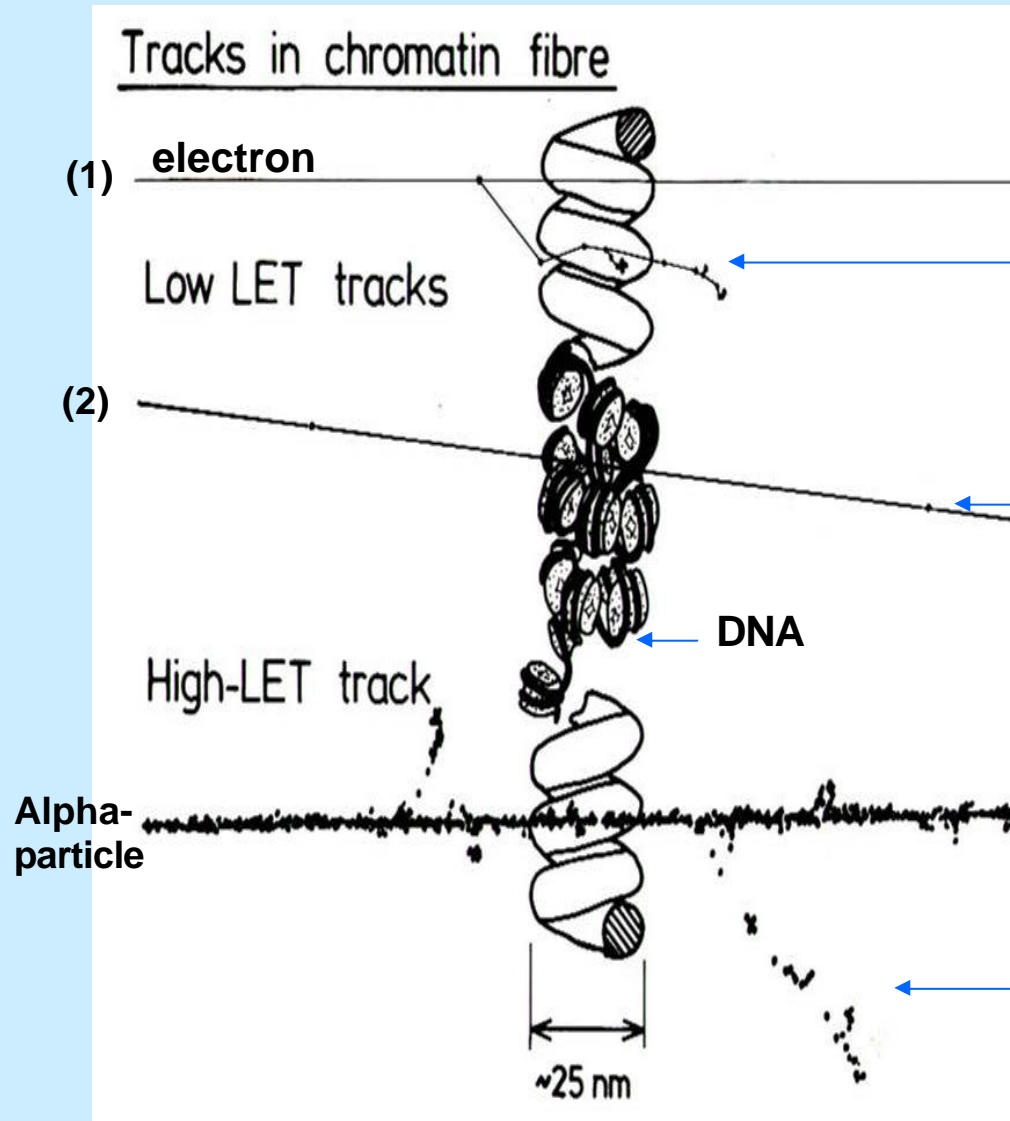
High-LET radiation:

Densely ionizing on average
(especially for low-velocity ions,
natural alpha-particles, etc)

High dose from a single track
($\sim 0.2 - 0.5$ Gy from single a-track)

LET = Linear Energy Transfer

All radiation tracks are highly structured on the scale of DNA



Clustered ionizations from low-energy electron

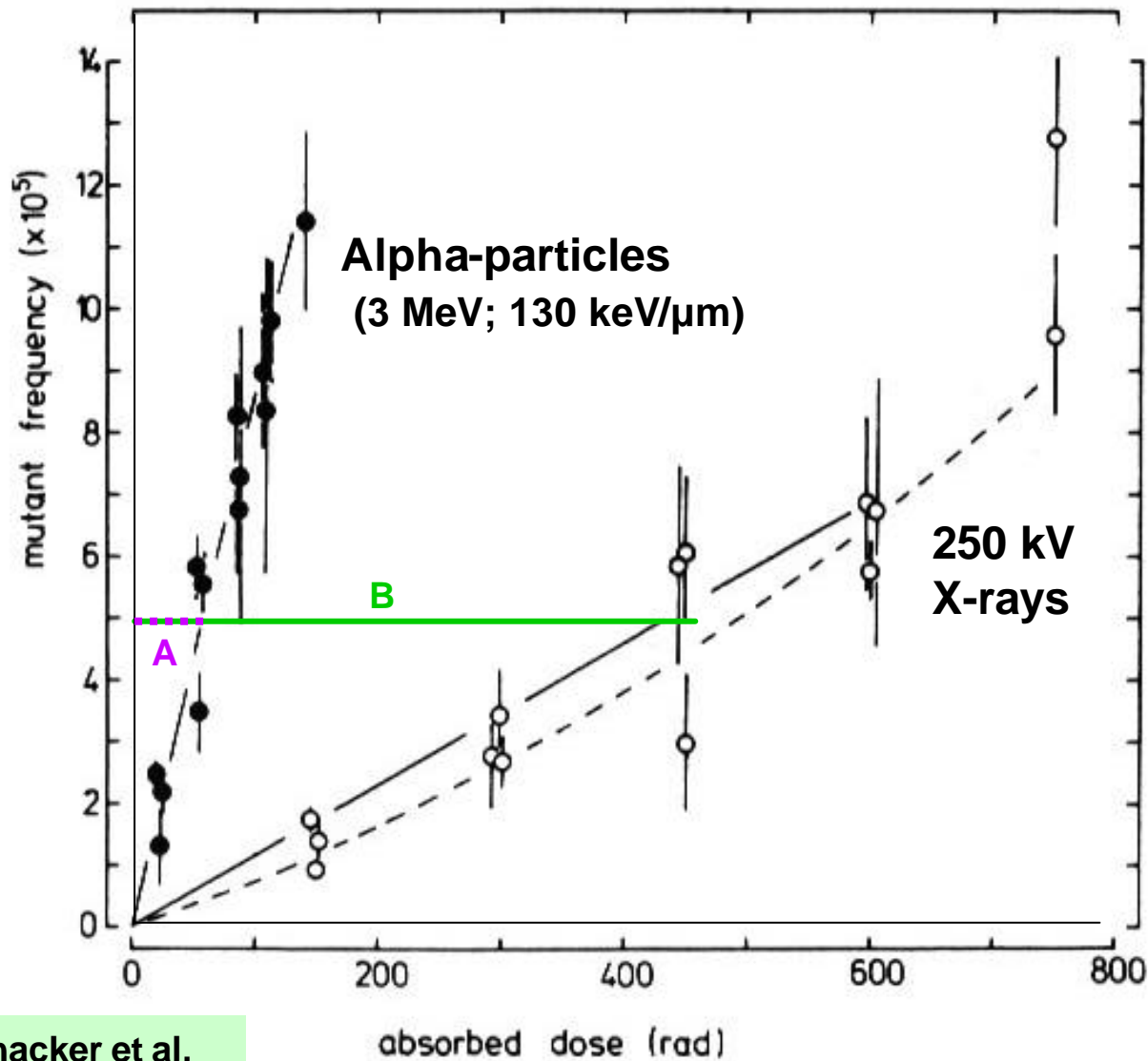
Single ionization

Opposing trends: Alpha-particle has -- low probability of hitting DNA (few tracks per Gy) -- high probability of damage when it does hit.

Delta-ray electron

Example:

**hprt mutation-induction by alpha-particles compared to X-rays
in V79 cells**



In general, biological effectiveness depends on:
--- radiation quality
--- dose
--- dose-rate
--- biological system

Here:

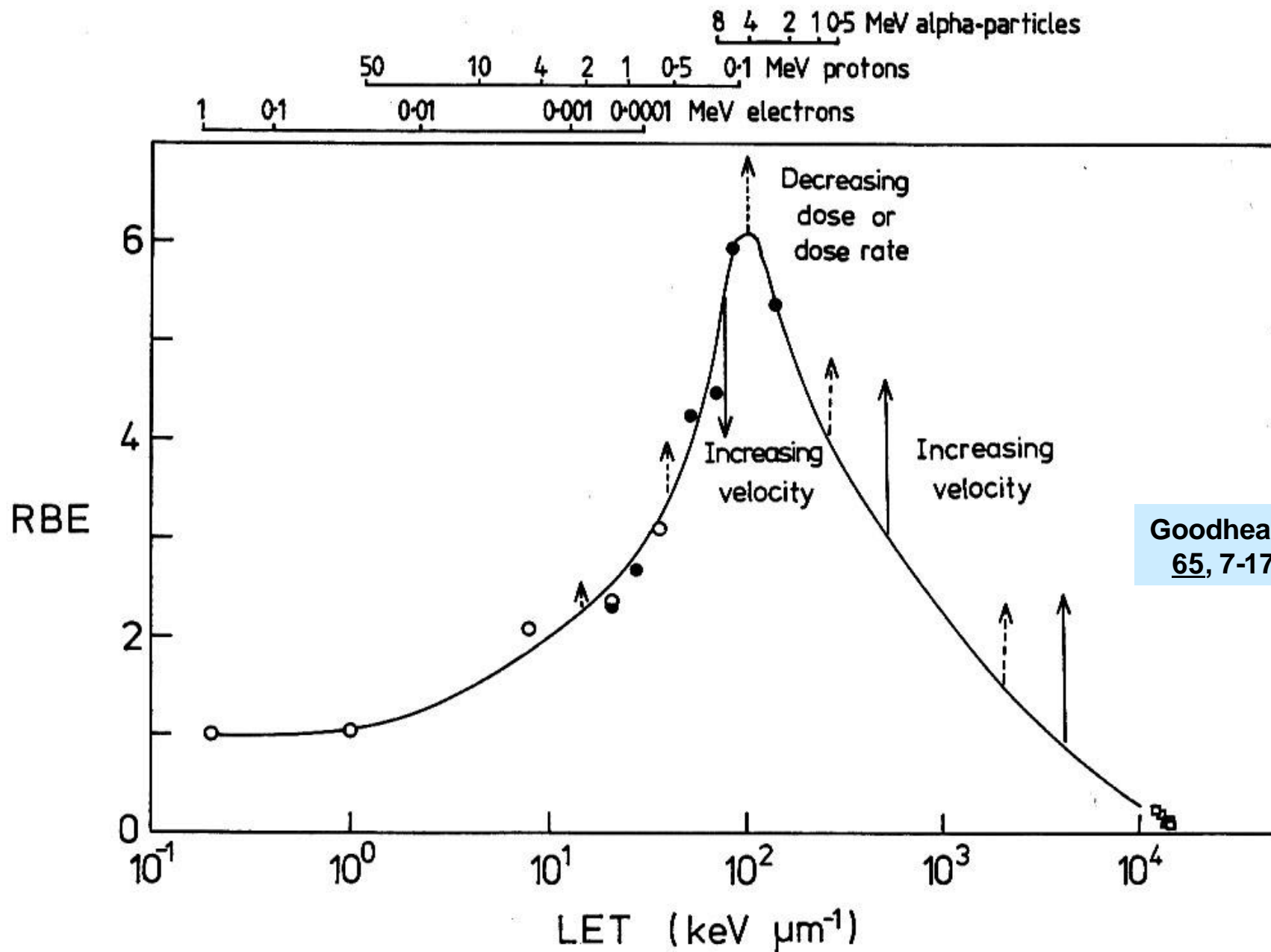
Relative Biological Effectiveness (RBE) of alpha-particles in this system is

$\frac{\text{Dose B}}{\text{Dose A}} \sim 8$

Thacker et al,
Radiat Res 92,
343-352 (1982)

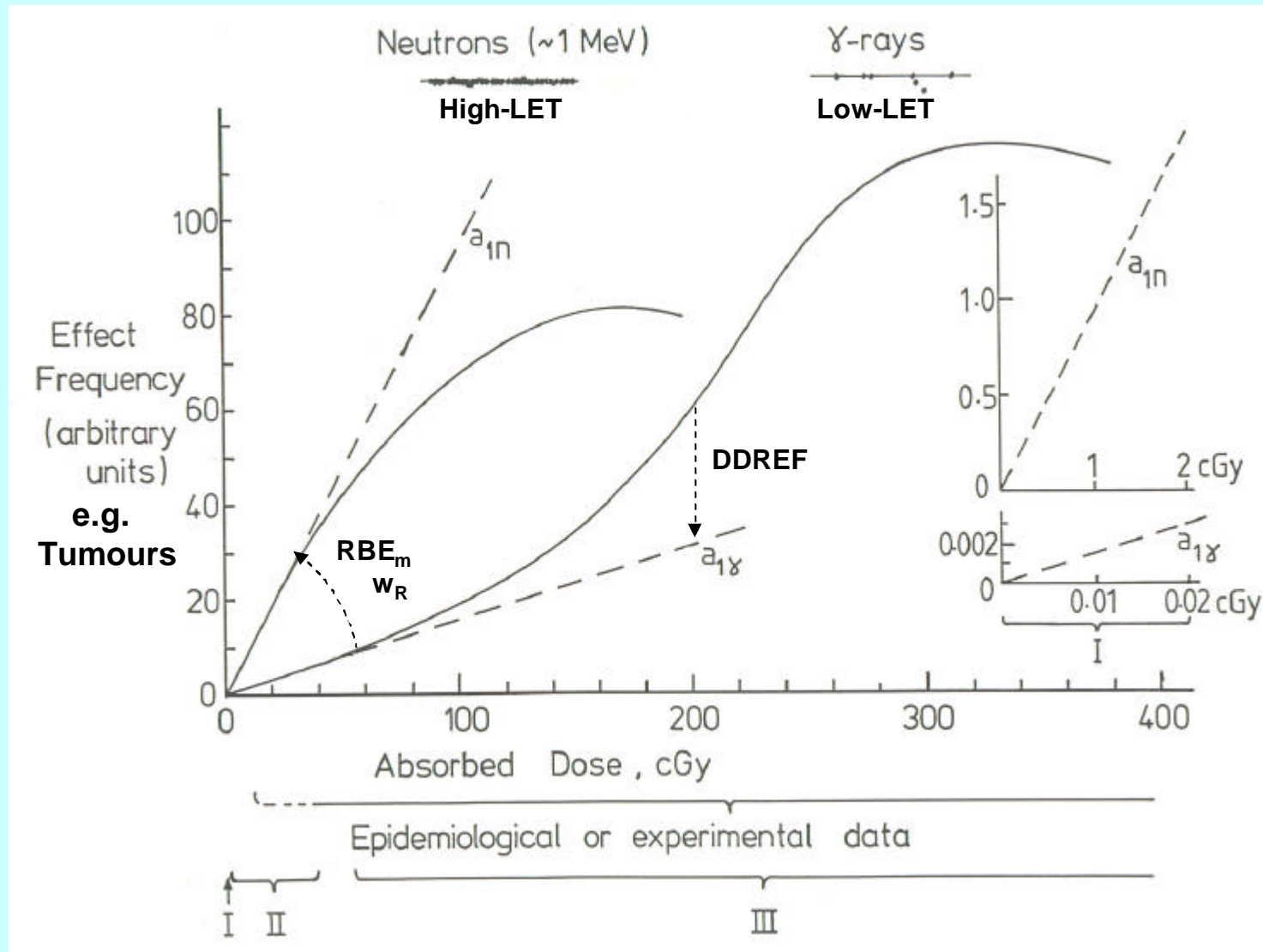
[100 rad = 1 Gy]

Relative Biological Effectiveness for Cell Inactivation by Ionizing Radiations



Goodhead, IJRB
65, 7-17 (1994)

Schematic dose responses for radiation risks



LET = Linear Energy Transfer
 RBE_m = Relative Biological Effectiveness (maximum)
 w_R = Radiation weighting factor
 DDREF = Dose and Dose-Rate effectiveness Factor

Mod from Goodhead, Adv
 Radiat Biol 16, 7 (1992)

ICRP system developed for radiation protection

Dosimetry/risk system based on

- Absorbed dose (D_T) to each tissue or organ Units: gray (Gy) = J/kg
(ie physical dose)
- but with 'subjective' prescribed weighting factors for approximate dependence of human risks:

(1) weighting for radiation quality:

Equivalent dose to a tissue,

$$H_T = S_R (w_R \cdot D_{T,R})$$

Units: sievert (Sv) = J/kg

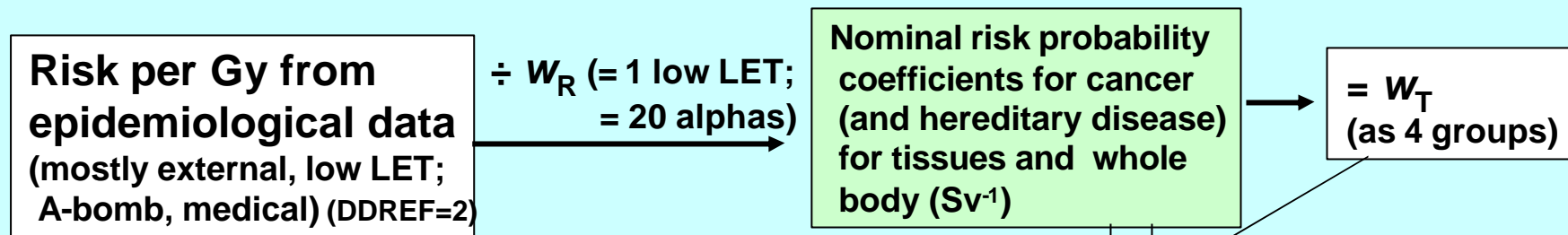
(2) weighting also for tissue sensitivity:

Effective dose to whole body,

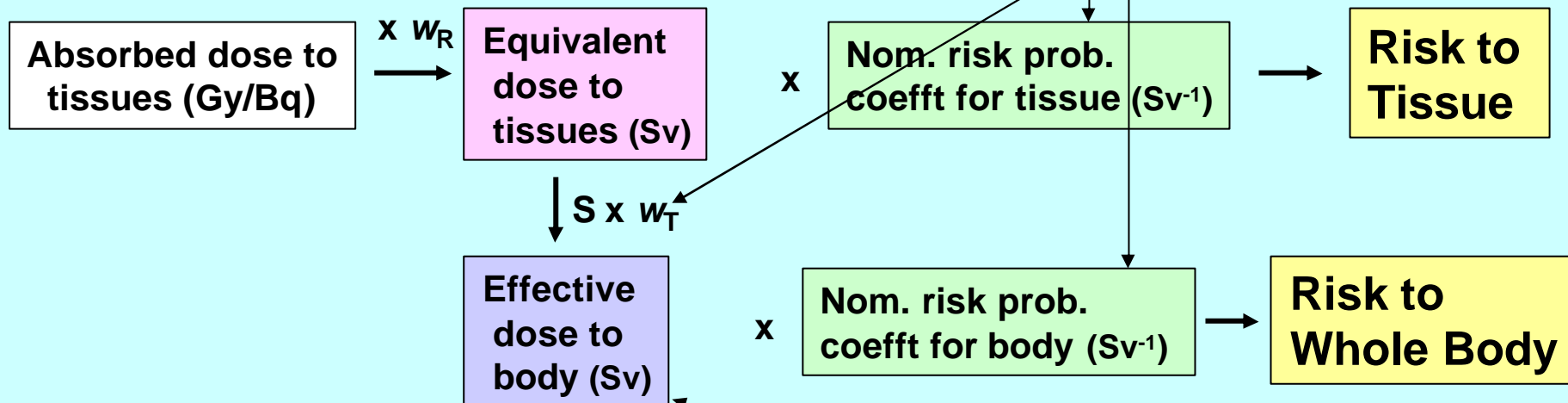
$$\begin{aligned} E &= S_T (w_T \cdot H_T) \\ &= S_{T,R} (w_T \cdot w_R \cdot D_{T,R}) \end{aligned}$$

Units: sievert (Sv) = J/kg

1. Primary ICRP risk estimates:



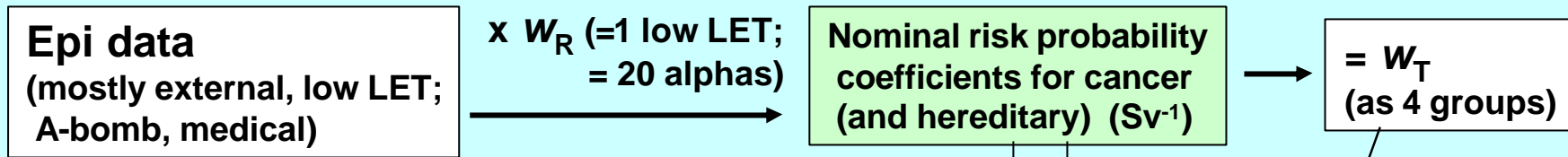
2. Hence, Estimated Risk for external radiation exposures:



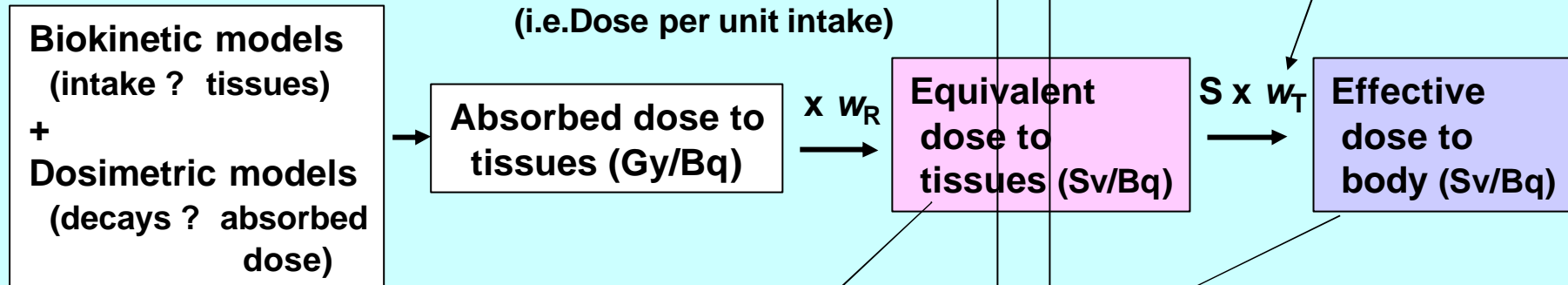
For radiation protection, limits are set in terms of effective dose (or equivalent dose) as surrogates for whole-body risk (or tissue risk).

Comment: Complex, yet crude, system to achieve additivity of risk from all exposures; Convenient for rough planning purposes in radiological protection.

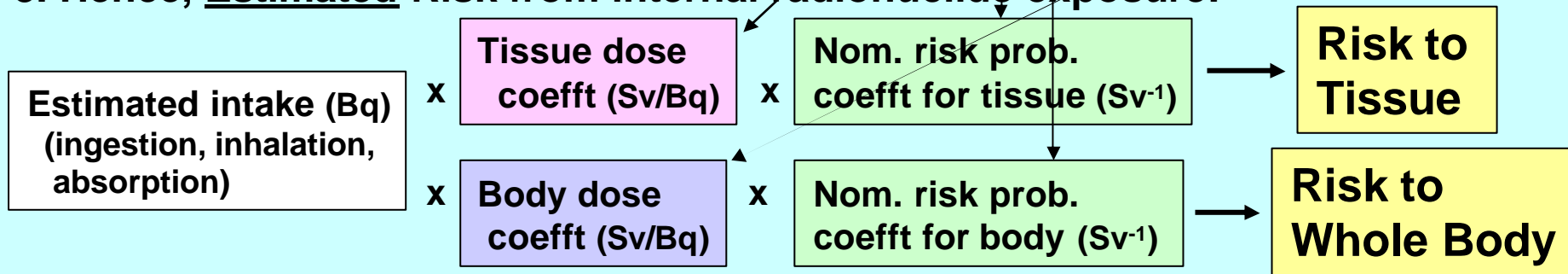
1. Primary ICRP risk estimates:



2. ICRP Dose Coefficients for internal radionuclides: (i.e. Dose per unit intake)



3. Hence, Estimated Risk from internal radionuclide exposure:



For radiation protection, limits are set in terms of effective dose (or equivalent dose) as surrogates for whole-body risk (or tissue risk)

Comment: Complex, yet crude, system to achieve additivity of risk from all exposures; Convenient for rough planning purposes in radiological protection.

Hence, effective dose is used

- as primary quantity for dose-limits in radiation protection
 - for prospective dose assessment, optimization and for demonstrating compliance
- as surrogate for risk (within the broad approximations of the ICRP system)
- for simple additivity of doses (and implied risks) from low-dose exposure scenarios, including
 - non-uniform irradiation of body or tissues
 - mixed radiation qualities
 - internal and external radiation sources
 - any temporal distributions of dose (i.e. dose-rate and dose fractionations)

Effective dose is not suitable for

- more accurate retrospective assessments of individual doses and risks
- use in epidemiological studies
- probability of causation in exposed individuals

[ICRP draft recommendations, Jan 2007]

Issues for this symposium could include:

- Appropriateness of ICRP specification of $w_R = 1$ for ALL photon and electron irradiations, including for low-energy beta emitters
- Under what circumstances should this value be used?
(e.g. prospective planning and routine records in radiation protection when doses are well below dose limits,)
- What values of RBE should be used for particular low-energy beta-emitters when more accurate dose or risk assessments are required?
(e.g. retrospective dose/risk assessments, prospective assessments/planning if approaching dose limits, epidemiology, compensation, litigation, ...)
- What other factors, in addition to radiation quality, may require consideration for particular low-energy beta-emitters?
(e.g. non-uniformity of absorbed dose to target cells within a tissue, to critical sub-cellular components, ...)
- Appropriateness of ICRP w_T values for ALL radiations, including low-energy beta emitters?

ICRP-prescribed values of radiation weighting factor

Radiation type and energy range

Radiation type and energy range	Prescribed w_R	
	ICRP(1991)	(ICRP2007 draft)
Photons, all energies	1	1
Electrons and muons, all energies	1	1
Neutrons, energy < 10 keV	5	Continuous fnc of energy, min 2.5, max 21
10 keV to 100 keV	10	
>100 keV to 2 MeV	20	
>2 MeV to 20 MeV	10	
>20 MeV	5	
Protons, other than recoil protons, >2 MeV	5	2
alpha particles, fission fragments, heavy nuclei	20	20

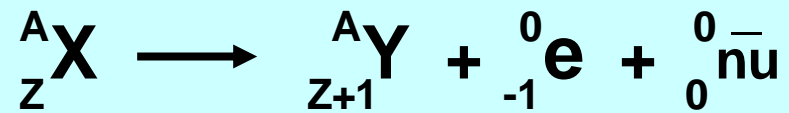
★ Implies equal risk per unit effective dose to body
per unit equivalent dose to a tissue
per unit absorbed dose to a tissue

For ALL photon and electron irradiations

ICRP treats: absorbed dose from low-energy beta emitters (few keV)
exactly as if from orthovoltage X-rays (~100 keV)
or from high-energy gamma-rays (~ 1 MeV).

Beta decay of radionuclides:

Electron emission (β^- decay):

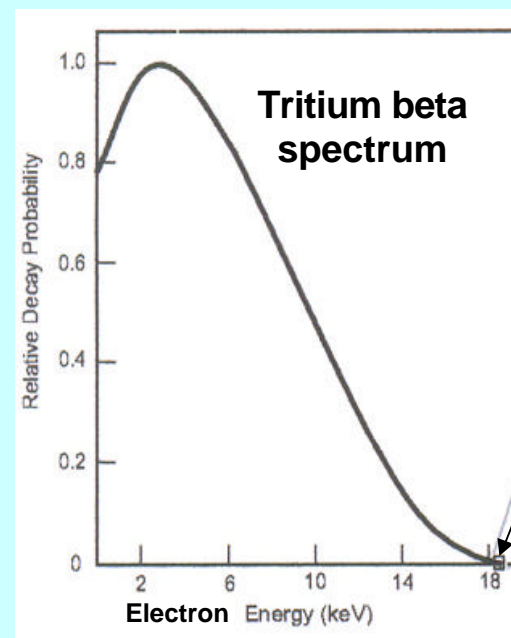
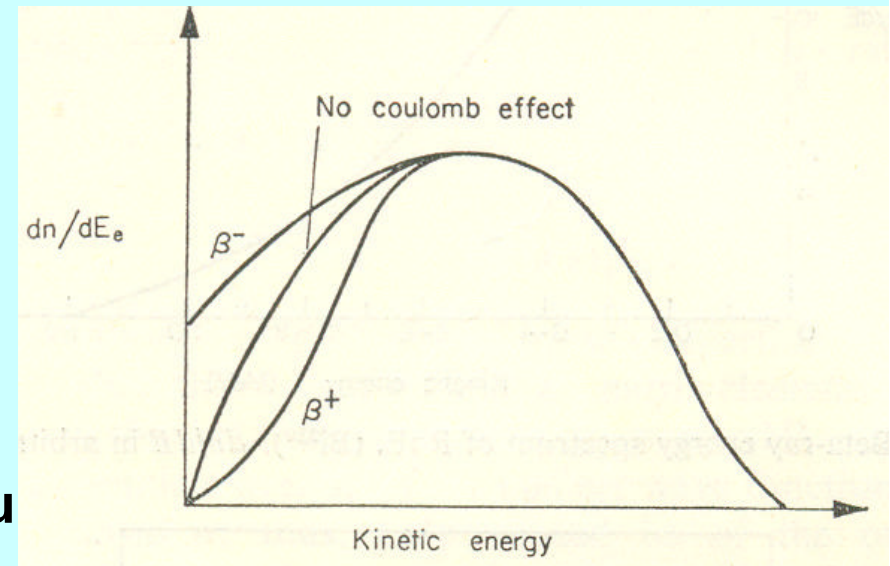
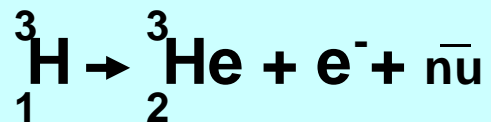


Positron emission (β^+ decay):



[where ν is neutrino]

Tritium β^- decay:



$$E_{\max} = 18.6 \text{ keV}$$

$$E_{\text{ave}} = 5.7 \text{ keV}$$

Some relevant low-energy beta⁻ -emitting radionuclides:

β^- -decay	Electron energy (keV)		Electron range (μm)		Half-life
	Max	Average	Max	Average	
${}^3_1\text{H} \rightarrow {}^3_2\text{He}$	18.6	5.7	~7	~0.56	12.3 y
${}^{14}_6\text{C} \rightarrow {}^{14}_7\text{N}$	157		~290		5730 y
${}^{35}_{16}\text{S} \rightarrow {}^{35}_{17}\text{Cl}$	167		~320		87 d
${}^{106}_{44}\text{Ru} \rightarrow {}^{106}_{45}\text{Rh}$	39.4		~28		574 d
${}^{210}_{82}\text{Pb} \rightarrow {}^{210}_{83}\text{Bi} \rightarrow (\beta, \alpha)$	63.5		~64		22 y
<u>Compare:</u>					
${}^{90}_{38}\text{Sr} \rightarrow {}^{90}_{39}\text{Y} \rightarrow (\beta)$	546		~1950		29 y
${}^{131}_{53}\text{I} \rightarrow {}^{131}_{54}\text{Xe} (+\text{gamma})$	971		~4200		8 d
${}^{137}_{55}\text{Cs} \rightarrow {}^{137}_{56}\text{Ba} (+\text{gamma})$	1176		~5200		30 y

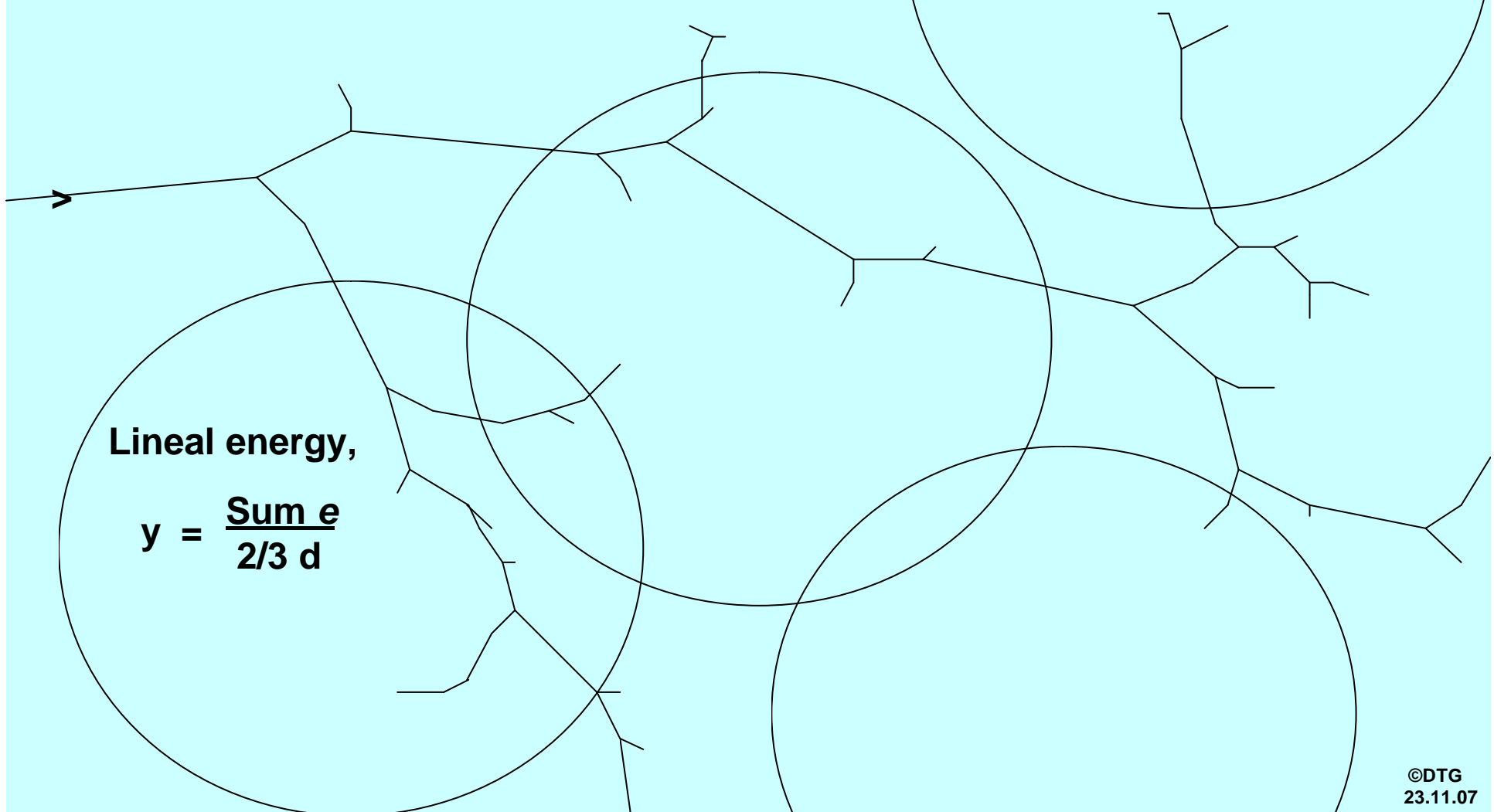
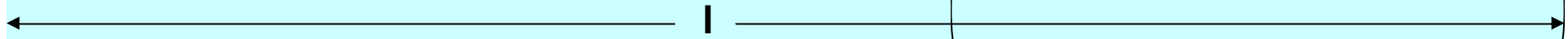
Unusual features of low-energy beta-emitters:

- 1) Increased average ionization density (LET)**
- 2) Short electron tracks**
- 3) Non-uniformity of dose**
- 4) Cell (or nucleus) hit frequencies per unit dose (numbers of tracks)**
- 5) Nuclear transmutations**
- 6) Isotopic mass differences**
- 7) Molecular forms**
- [8) Positron annihilation for β^+ -emitters]**

Most of these features are not incorporated into conventional radiation protection dosimetry.

Average Linear Energy Transfer (LET), $L = \frac{\text{Sum } e}{\bar{I}}$

Average energy restricted LET, $L_{\text{Delta}} = \frac{\text{Sum}(e < \text{Delta})}{\bar{I}_{\text{total}}}$



Lineal energy,

$$y = \frac{\text{Sum } e}{2/3 d}$$

Unusual features:

1) Increased average ionization density on subcellular scale
(by whatever measure)

		X-rays			⁶⁰ Co gamma
		Tritium β	50kV	250kV	
<u>LET (Linear Energy Transfer) (keV/μm)</u>					
Track-average LET ($\bar{L}_{100,T}$) [$L_{8,T}$]		4.7 [~12]	6.3	1.7	0.22
Dose-average LET ($\bar{L}_{100,D}$) [$L_{inf,D}$]		11.5	13.1	9.4	6.9 [0.31]
<u>Lineal energy (keV/μm)</u>					
Site diameter d = 5 μm	Frequency-mean (\bar{y}_F) Dose-mean (\bar{y}_D)	1.4 2.1	65kV ~1.7	200kV 1.0	0.28 0.62
d = 1 μm	Frequency-mean (\bar{y}_F) Dose-mean (\bar{y}_D)	3.1 5.2	2.2 5.0	1.2 3.7	0.37 1.6
d = 0.5 μm	Frequency-mean (\bar{y}_F) Dose-mean (\bar{y}_D)	4.1 7.3	2.6 5.4	1.4 4.7	0.52 2.3
d = 0.1 nm	Frequency-mean (\bar{y}_F) Dose-mean (\bar{y}_D)	4.0 9.2	40kV -	250 kV -	- 4.3
d = 0.01 nm	Frequency-mean (\bar{y}_F) Dose-mean (\bar{y}_D)	7.8 18.0	6.9 17.7	6.1 17.0	- 12.6

Unusual features:

1) Increased average ionization density on subcellular scale
(by whatever measure)

LET (Linear Energy Transfer)

Track-average LET ($\bar{L}_{100,T}$) (keV/ μm)

Dose-average LET ($\bar{L}_{100,D}$) (keV/ μm)
($\bar{L}_{\text{inf},D}$) (keV/ μm)

	Tritium β	X-rays		^{60}Co gamma
		50kV	250kV	
Track-average LET ($\bar{L}_{100,T}$) (keV/ μm)	4.7	6.3	1.7	0.22
Dose-average LET ($\bar{L}_{100,D}$) (keV/ μm)	11.5	13.1	9.4	6.9
($\bar{L}_{\text{inf},D}$) (keV/ μm)				0.31

Compare with protons of similar LET:

~ 10 MeV protons have LET (L_T) = 4.7 keV/ μm

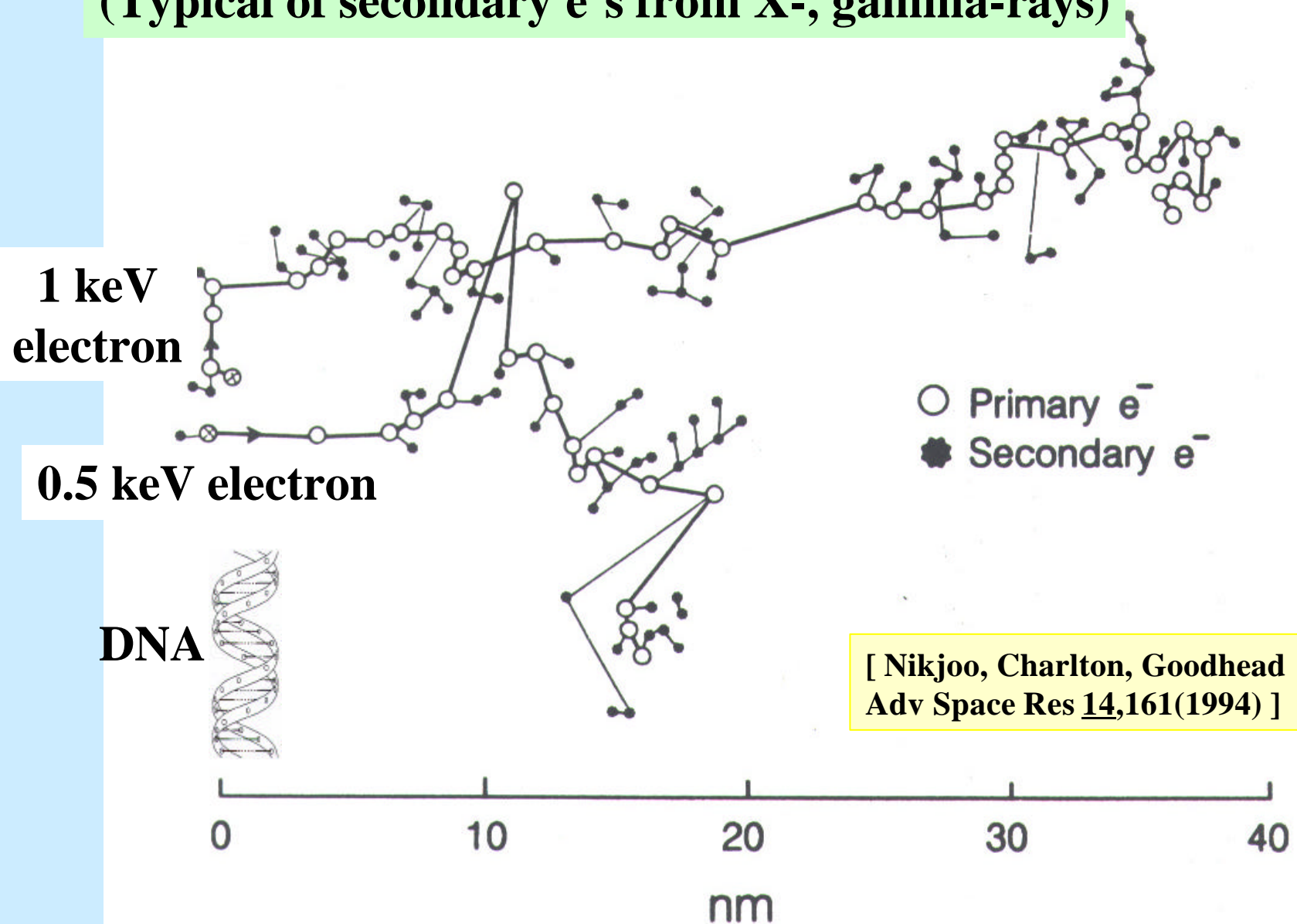
For protons ICRP prescribes $w_R = 5$ (ICRP60, 1991)

= 2 (ICRP draft recs, Jan 07)

(reduced partly on the basis of low penetration of external protons)

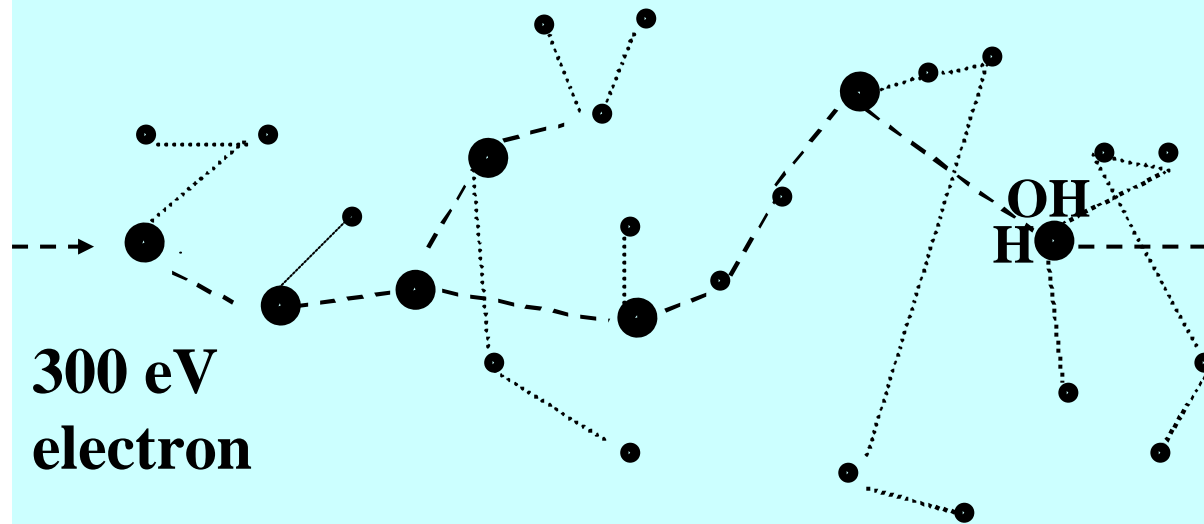
Two low-energy-electron tracks

(Typical of secondary e's from X-, gamma-rays)



Clustered DNA damage

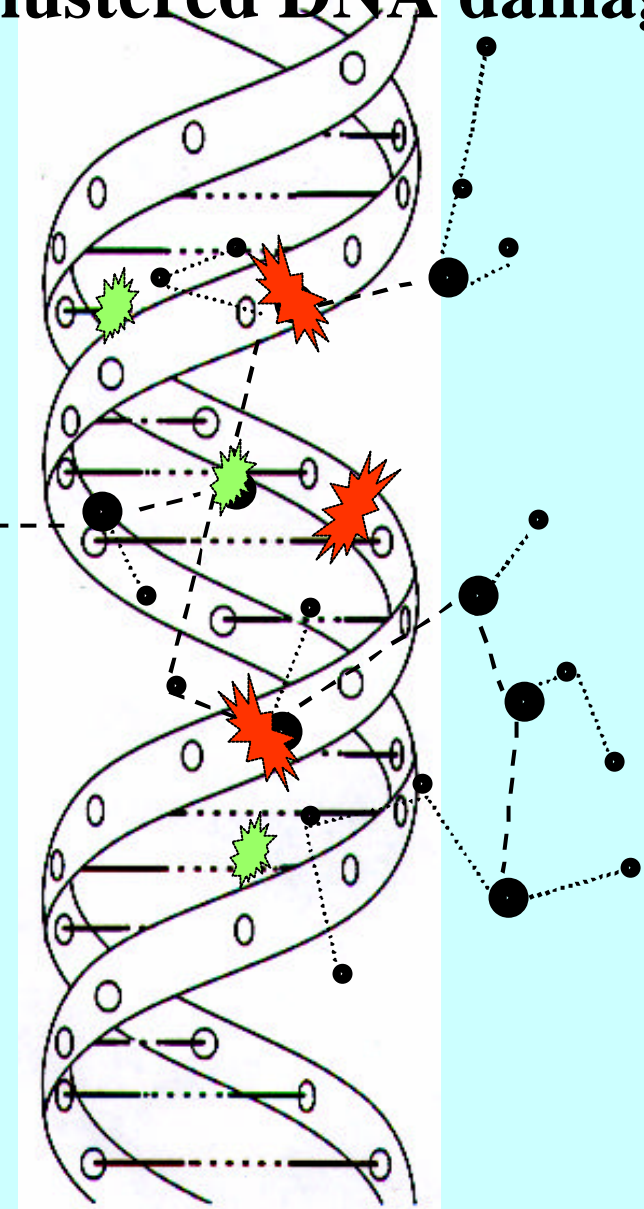
Electron track



300 eV
electron

- = ionized molecule
- = excited molecule

2 nm



Unusual features:

2) Short ranges of electrons (beta-particles)

Ranges of tritium beta-particles:

Average 0.56 μm
Maximum ~ 7 μm

Compare with:

Typical cell diameters	~ 7 μm to 30 μm
Typical cell nucleus diameters	~ 6 μm to 15 μm
Chromatin fibre diameter	~ 0.030 μm
DNA diameter	~ 0.0024 μm

Hence:

Short range

- does not mask increased LET of these electrons on scale of DNA and chromatin;
- limits ability of single track to damage two distant targets on cellular scale;
- can lead to non-uniformity of dose when emitters are inhomogeneously distributed.

Unusual features:

3) Non-uniformity of absorbed dose

Occurs when β -emitters are non-uniformly distributed on scales of:

- tissue compartments (all low-energy β -emitters)
- individual cells (some low-energy β -emitters)
- cell compartments, eg nucleus vs cytoplasm
(a few low-energy β -emitters)
- chromosomes or DNA (notably tritium)

Examples: Tritiated DNA precursors;
OBT in adipose tissue;
.....
etc

NOTE: Also, mean ionization density may be increased in targets with bound tritium compared to uniform HTO. [Chen (2006): \bar{y}_D ratio ~ 1.7]
Additional to enhancement of absorbed dose.

Unusual features:

4) Cell (or nucleus) hit frequencies per unit dose

- Larger mean energy deposition by single ^3H β than from single track from Co gamma;
- Hence, fewer hits from tritium than from Co gamma-rays (for equal average absorbed dose to tissue);
- i.e. Fewer cells (or nuclei) are hit by ^3H , but they are hit harder.
- Any consequences? (Thresholds, Dose rate)

		^3H	Co gamma
For sphere $d = 7 \mu\text{m}$	\bar{z}_F (mGy)	4.6	1.1
	<u>Hit frequency</u> $= 1/\bar{z}_F$ (mGy $^{-1}$)	0.2	0.9
For sphere $d = 12 \mu\text{m}$	\bar{z}_F	1.3	0.4
	<u>Hit frequency</u> $= 1/\bar{z}_F$ (mGy $^{-1}$)	0.8	2.5

where \bar{z}_F = mean specific energy

Unusual features:

5) Nuclear transmutation

- Molecular changes result from transmutation of β -emitting radionuclide
- Conversion of ^3H to ^3He loses its chemical binding in molecule
(e.g. deprotonation in a DNA base, potentially mutagenic?
disruption of hydrogen bonding in DNA)
- Conversion of ^{14}C to ^{14}N in DNA base (potentially mutagenic?)
- Conversion of ^{35}S to ^{35}Cl alters the biomolecule

Unusual features:

6) Isotopic mass difference ratio compared to stable isotope

- Affects physico-chemical properties
- Mass difference is very large for ^3H compared to normal ^1H ,
by ratio of 3
(e.g. affect chemical reaction rates for uptake and clearance;
differential diffusion;
'buried tritium':
differential binding of water in hydration shell of DNA – enrichment factor 2?
differential binding in proteins, other macromolecules -- " " 1.4?
- Ratios are very small for most other β -emitters

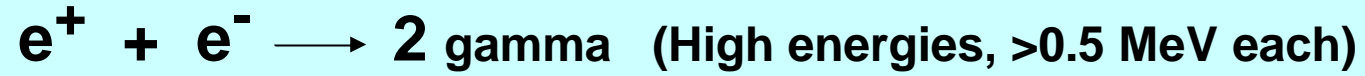
Unusual features:

7) Molecular forms

- Different molecular compounds of β -emitters can influence uptake ratios, retention times and other biokinetic parameters
- Notable forms for ^3H include:
 - tritiated water
 - organically bound tritium (OBT) – exchangeable
 - non-exchangeable
 - DNA precursors

Unusual features:

8) Positron annihilation (β^+ emitters)



- Delocalizes energy of β^+ -emitters

Unusual features of low-energy beta-emitters:

- 1) Increased average ionization density (LET)
- 2) Short electron tracks
- 3) Non-uniformity of dose
- 4) Cell (or nucleus) hit frequencies per unit dose (numbers of tracks)
- 5) Nuclear transmutations
- 6) Isotopic mass differences
- 7) Molecular forms

[8) Positron annihilation for β^+ -emitters]

- Most of these features are not incorporated into conventional radiation protection dosimetry.
- They may be incorporated in various ways into experimental measurements of RBE

A few additional comments

Comment

Low-energy electrons are an important component for dose deposition by all low-LET radiations (X, gamma, e);
But especially so for tritium β -decay.

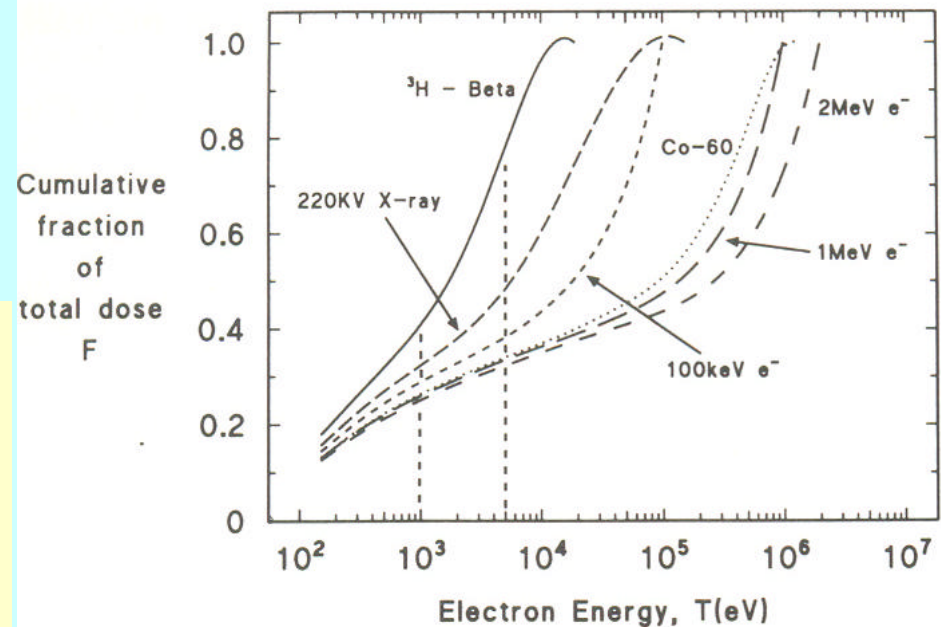
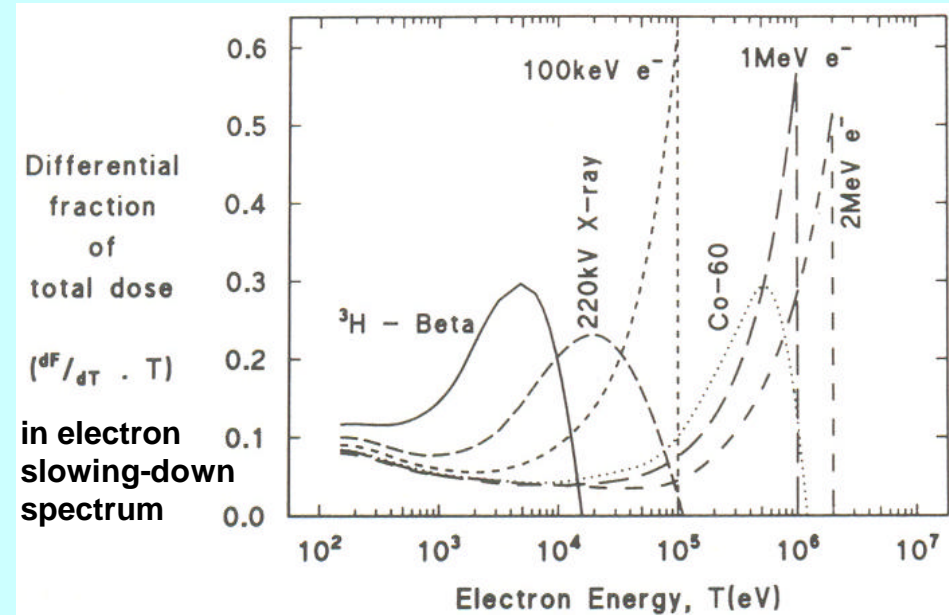
COMPARE:

Dose fraction deposited by electrons of energies 0.1 to 5 keV

from:	Tritium β	77 %
	220 kV X-rays	38 %
	Co gamma rays	34 %

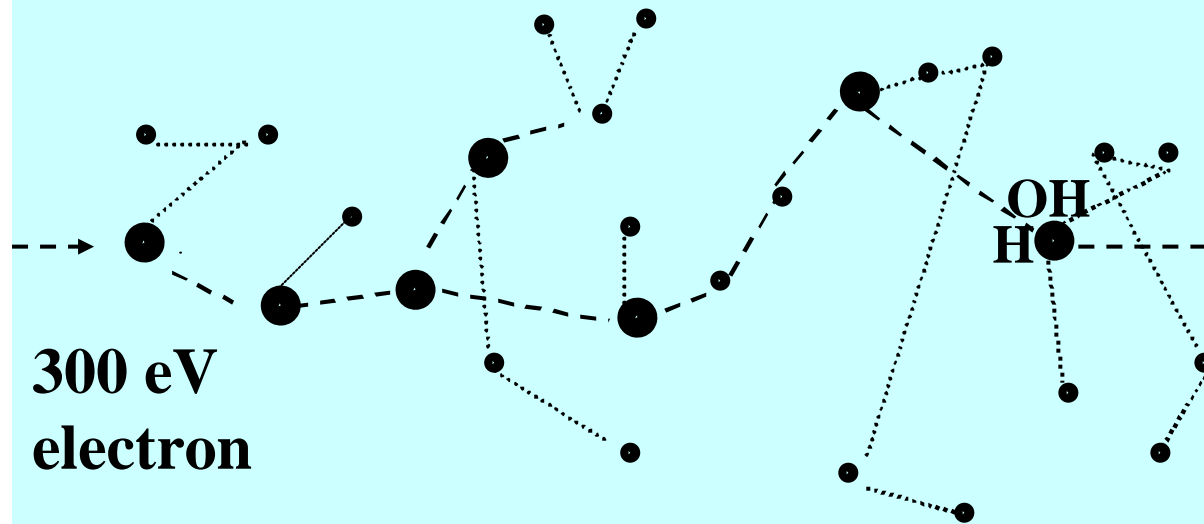
NOTE: Low energy electrons are more efficient at:

- producing DNA double-strand breaks (DSB)
- producing a higher proportion of complex DSB (and other clustered damage)



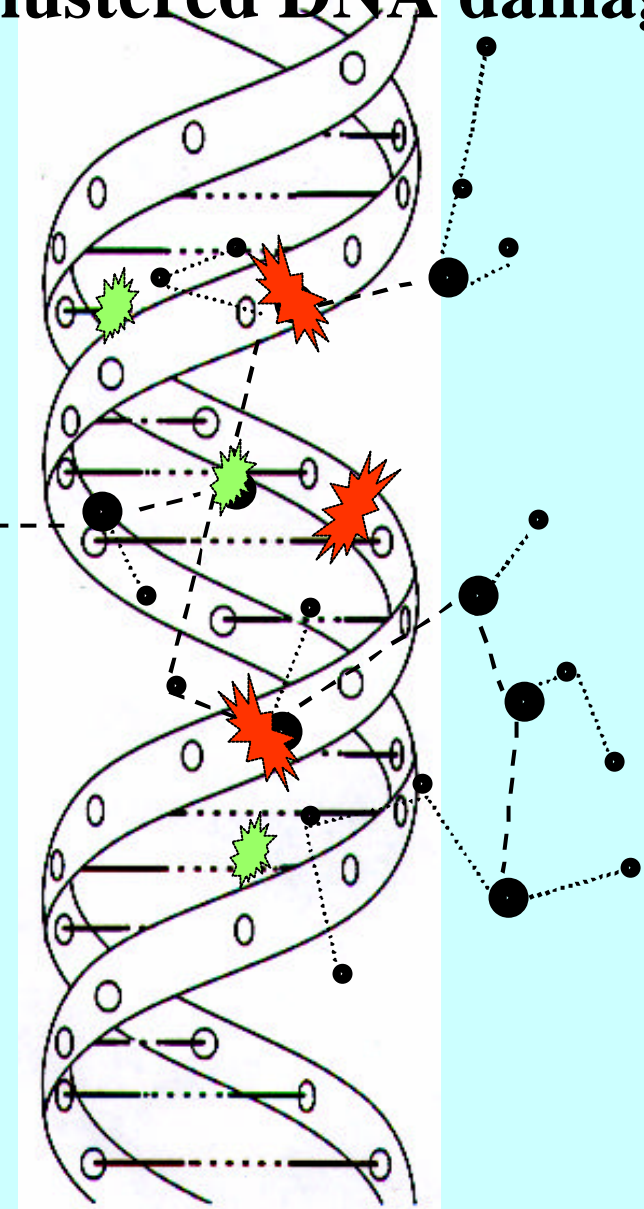
Clustered DNA damage

Electron track



- = ionized molecule
- = excited molecule

2 nm



Complexity of DNA Strand Breaks

**E
L
E
C
T
R
O
N
S**

Energy keV	% No Break	SSB %	SSB+ %	2SSB %	DSB %	DSB+ %	DSB++ %	SSB Complex Total	DSB Complex Total	SS DS
0.1	73.9	22.4	1.86	0.09	1.39	0.27	0.015	8.0%	17%	17
0.3	66.4	26.6	3.29	0.43	2.38	0.85	0.092	12.3%	28%	11
0.5	68.7	25.4	2.78	0.47	1.86	0.79	0.070	11.3%	29%	13
1.0	68.9	25.2	2.75	0.50	1.81	0.71	0.081	11.4%	32%	13
1.5	70.5	24.3	2.39	0.40	1.68	0.63	0.074	10.3%	29%	14
4.5	80.6	17.6	0.90	0.18	0.52	0.17	0.013	5.8%	26%	26
10	81.1	17.4	0.78	0.13	0.47	0.13	0.014	5.0%	23%	30
20	81.3	17.2	0.75	0.12	0.46	0.13	0.012	4.8%	23%	30
50	81.8	16.9	0.70	0.12	0.44	0.12	0.009	4.6%	22%	31
100	81.8	16.9	0.60	0.11	0.47	0.11	0.008	4.1%	20%	30

a

MeV	
4.0	58.1 25.0 6.1 1.28 3.76 3.86 1.90 23 % 61% 3
2.0	53.3 23.1 6.8 1.90 4.01 6.14 4.81 27 % 73% 2

Nikjoo/Goodhead/O'Neill/Terrissol/Wilson/Bolton/Watanabe: IJRB 71,467('97); Rad Res 148,485('97) & 156,577('02); Rad Prot Dosim 99,77('02)

Comment

Table commonly referred to as justification for claim of RBE = 2 of orthovoltage X-rays compared to ^{60}Co gamma rays!! (eg ICRP60)

Table D-3--- Low Dose RBE studies of Low-Let Radiation^a
(Bond et al 1978)

System	Radiation	RBE = alpha ratio	(Table copied from ICRU40, 1986)
<i>Tradescantia</i> stamen hair mutation	X gamma	2.1	
Lymphocyte chromosome aberrations	X e	3.2	
Mouse oocyte killing	^3H gamma	2.9-4.2	

^aEffect = $\alpha \cdot D + \beta \cdot D^2$, RBE is equivalent to RBE_M

- Very poor justification!!

Lymphocyte dicentric aberrations remain the mainstay of such claims, with heavy reliance on simple curve-fitting extrapolations.

Conclusions

- **General expectation that low-energy beta emitters will have greater biological effectiveness than standard reference radiations**
Supported from many directions, experimental and theoretical.
- **The magnitude and practical implications need consideration.**
- **Some special features of low-energy beta emitters may be overlooked in routine RBE experiments**
- **There may be issues with use of standard tissue weighting factors for all low-energy beta emitters**
e.g. access to target cells, or excesses therein
(radiation quality differences)

Some recommendations

- Use available information (experimental and theoretical) to establish the likely effectiveness of low-energy beta emitters for human risk relative to reference radiations
- Consider special cases of potential practical relevance
e.g. extreme inhogeneity
- Determine yields and complexity of DNA damage from tritium beta-emitters, including when bound to cellular DNA, in comparison with a reference radiation
- Seek agreement on a standard reference radiation of practical convenience and relevance to established human risks

THE END